
REVIEW ARTICLE

Transfersomes As Promising Lipid Based Nanocarrier Tool in Novel Drug Delivery System

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ABSTRACT

Novel drug delivery system are nowadays is creating a new interest in development of drug deliveries vesicular drug delivery system. It is a part of novel drug delivery system. The barrier function of the skin typically restricts the transdermal delivery of medications. One of the more contentious approaches to the transdermal distribution of active ingredients involves vesicular networks. The discovery of elastic vesicles like transfersomes, etc. rekindled interest in developing transdermal delivery systems. It can improve the therapeutic efficacy and safety of the drugs because drug delivered through the skin at a predetermined and controlled rate. Due to the flexible nature of the stratum corneum, transfersomes can pass through pores that are smaller than it and enter the underlying living skin in intact form. Drugs of both low and large molecular weights, including analgesics, anaesthetics, corticosteroids, anticancer, insulin, gap junction protein, and albumin, can be transported via them. These delivery systems were conceptualised in an effort to concentrate the medicine in the target tissues while decreasing the amount of drug in the non-target tissues. As a result, the medication has no effect on the tissues nearby. Additionally, localisation prevents medication loss from occurring leading to the medication's greatest effectiveness. As a result, the phospholipid-based carrier systems are very interesting today and the advantages of transfersomes i.e., improved bioavailability and longer duration of action which result in a reduction of dosing frequency

Keywords: Transfersomes, Novel drug delivery, Transdermal drug delivery.

Received 24.08.2023

Revised 21.09.2023

Accepted 17.12.2023

How to cite this article:

Aman A, Upendra Singh B, Nitin D. Transfersomes As Promising Lipid Based Nanocarrier Tool in Novel Drug Delivery System. Adv. Biores., Vol 12 (6) November 2023: 467-476.

INTRODUCTION

The novel drug delivery system is referred to be a rebirth system since it has updated a number of drugs and assisted in overcoming several drug-related issues, allowing us to use longer-acting pharmaceuticals with controlled activity. There has been significant progress in the development of a number of novel drug delivery techniques. The novel drug delivery system is the most appropriate and approachable in developing a delivery system that improves the therapeutic efficacy of new and conventional drugs that provides controlled and sustained drug delivery to a specific site and meets appropriate drug concentration in body. It has the ability to deliver medication to a precise site of action. One such strategy that can be predicted to prolong the drug residence in systemic circulation while minimising its toxicity is encapsulation of the drug in vesicular structures. Since then, advancements in vesicular drug delivery have resulted in the development of systems that enable drug targeting and the extended or controlled release of conventional therapies. The stability of the vesicular system is significant because of the formation of vesicles.[1]

NOVAL DRUG DELIVERY SYSTEM

The phrase "novel drug delivery system" (NDDS) refers to the development of new pharmacological forms with advantageous qualities such as smaller particle size higher permeability parameters, and selective site targeting. NDDSs can be used to increase the performance of biotherapeutic medications when compared to their impact in typical dosage forms. A complex drug delivery system developed to maximize therapeutic impact and manage medication release is known as an innovative drug delivery system. The concept of a

New Drug Delivery System (NDDS) motivated researchers to create a novel, innovative, and one-of-a-kind drug delivery system or practice of injecting or administering a pharmacological substance into systemic circulation to achieve its therapeutic impact in humans or animals. The manner in which a medication is delivered can have a significant influence on its efficacy. Several drugs have a concentration range that is ideal. Maximum benefit is gained at dosages within this range, but amounts outside of this range might be hazardous or provide no therapeutic benefit. On the other hand, the slow progress in the efficacy of severe sickness therapy has highlighted a growing need for a multimodal strategy to therapeutic administration to tissue targets. This led to the development of innovative approaches for controlling pharmaceutical pharmacokinetics, pharmacodynamics, non-specific toxicity, immunogenicity, biorecognition, and efficacy. These novel drug delivery systems (DDS) are based on interdisciplinary approaches that combine polymer science, pharmaceuticals, bioconjugate chemistry, and molecular biology to decrease pharmaceutical degradation and loss, eliminate unwanted side effects, and enhance drug bioavailability and drug fraction.[2][3]

In general, the pharmaceutical drug delivery system is made by

1. A suitable dosage form (pharmaceutical formulations) for delivering the drug to the body
2. Following delivery, a drug release mechanism from the dosage form to the organ/cells of targeting
3. The dosage form is manufactured using the best medical device/pharmaceutical technologies available.

As a result, a Novel drug delivery system might be created by:

1. Developing SMART nanocarrier-based drug delivery devices to improve cell selectivity.
2. Improved control over the duration of effect (SMART extended-release drug delivery systems).
3. Application of novel manufacturing methods, such as microfluidics (MF).

NOVEL DRUG DELIVERY FORMULATION

Liposomes

Liposomes are small vesicles made up of lipid bilayers that are similar to cell membranes in structure. They have a spherical form and can range in size from 10-100nm in diameter. The term "liposome" is derived from the words "lipid" and "soma" (which means "body"). Liposomes have a wide range of applications, including medications, cosmetics, and research. Because of their capacity to encapsulate and transport both hydrophilic (water-soluble) and hydrophobic (fat-soluble) molecules, they are typically used as drug delivery systems. The hydrophilic chemicals are contained within the aqueous core of liposomes, whereas the hydrophobic substances are contained within the lipid bilayer. Liposomes' structure protects encapsulated chemicals from degradation, improves their stability, controls their release, and improves their bioavailability. Liposomes are valuable for targeted medicine administration because they may be tailored to target certain tissues or cells. They can also be changed to increase the duration they spend in the bloodstream or to improve their absorption by cells. Liposomes are used in cosmetic compositions, where they can encapsulate active substances such as vitamins or antioxidants, assisting in their transport to the skin. Liposomes are also utilized as model systems in molecular biology and research to examine membrane characteristics, drug interactions, and biological processes. Liposomes, in general, provide flexible and promising platforms for drug administration and other uses with continuous research targeted at optimizing their characteristics and discovering novel therapeutic potential.[3],[4],[5]

Nanoparticle

Nanoparticles are particles that range in size from 1 to 100 nm. These particles can be made of a variety of materials, including metals, ceramics, polymers, and composites. Nanoparticles have unique features that distinguish them from their bulk counterparts due to their tiny size. A high surface-to-volume ratio, higher chemical reactivity, and changed optical, magnetic, and electrical properties are among these traits. These properties make nanoparticles application in a variety of sectors, including medicine, electronics, energy, and environmental science.[6]

Niosomes

Niosomes are multilamellar vesicles composed of non-ionic surfactants of the alkyl or dialkyl polyglycerol ether family and cholesterol. Earlier research, conducted in collaboration with L'Oreal, showed that niosomes, in general, have capabilities as potential drug carriers comparable to liposomes. Niosomes vary from liposomes in that they have specific benefits over liposomes.[7]

Proniosome

The proniosome gel system is a step ahead of niosome, which may be used for a variety of applications in the delivery of actives to the desired place. Proniosomal gels are formulations that, when hydrated in situ with skin water, transform into niosomes.

Solid Lipid Nanoparticles (SLN)

It is a technology that was created in the 1990s. It is a colloidal carrier that is specifically designed for the transport of lipophilic chemicals. The typical mean size of solid lipid nanoparticles spans between 50 and 1000 nanometers. Solid lipid nanoparticles are made of a lipid matrix that solidifies at ambient temperature and also at body temperature. The primary advantages of solid lipid nanoparticles (SLNs) for parenteral administration are their exceptional physical stability and the preservation of integrated labile pharmaceuticals from degradation. It should be made for the selection of lipids and surfactants to pass the blood-brain barrier. SLNs are made using a variety of techniques, including homogenization, warm micro-emulsion high-speed stirring ultrasonication, and solvent diffusion. Lipids are compatible with lipophilic medicines and boost their efficacy.

Spanlastics

Spanlastics are a new drug delivery device that entraps the medication in the core cavity as a bilayer. In 2011, the name Spanlastic (Span + Elastic) was invented for the first time. Similar to transfersomes, these are extremely malleable and elastic carriers. In comparison to medication solution, these deformable vesicular carrier systems have higher permeability. These are amphiphilic in nature, with the drug enclosed in a vesicle formed by a non-ionic surfactant. The spanlastics are exceedingly little and microscopic. These are a subset of nanovesicles that overcome the shortcomings of liposomes, such as chemical instability. Its chemical instability is caused by their proclivity for oxidative breakdown and fluctuating phospholipid purity.[7]

TRANSFERSOMES

Transfersomes are lipid-based nanocarriers that are utilized to transfer medications or other bioactive compounds. They are intended to improve drug absorption and bioavailability by enhancing drug penetration via the skin or mucosal membranes. Transfersomes, like liposomes, are made of phospholipids, but they have special features that allows them to bend and squeeze through small holes, such as the intercellular gaps of the skin. Transfersomes flexibility and deformability allow them to carry drug to deeper layers of the skin or over other barriers. Transfersomes have a bilayer membrane made of phospholipids and an aqueous core that envelopes the drug or API. Because of this, transfersomes may transport both hydrophilic (water-soluble) and lipophilic (fat-soluble) drug. Transfersomes can be used for a variety of purposes, including transdermal drug administration, which allows pharmaceuticals to be absorbed via the skin for systemic distribution. They have demonstrated promise in the delivery of medications for illnesses like as skin cancer, psoriasis, and other dermatological problems. Furthermore, by changing their surface features and integrating targeting ligands transfersomes can be used for targeted drug delivery to specific tissues or organs. While transfersomes have showed promise in drug delivery, further research and development is needed to optimize their formulation, stability, and therapeutic uses.

Advantages of Transfersomes

- **Increased skin penetration:** Transfersomes can penetrate the stratum corneum, the outermost layer of skin, more successfully than conventional drug delivery methods. This enables more effective medication and therapeutic agent administration into the deeper layers of skin.
- **Flexibility and deformability:** Transfersomes are lipid vesicles that are very flexible and malleable. They can readily pass through small pores and penetrate the natural barrier of skin. Because of their adaptability, transfersomes may encapsulate a diverse spectrum of therapeutic molecules, including both hydrophilic and lipophilic substances.
- **Enhanced drug bioavailability:** Because Transfersomes are malleable, they can more easily penetrate the protective barriers of skin, such as the stratum corneum and epidermal layer
- **Transfersomes can be modified on the surface with ligands or antibodies to enable targeted medication delivery.** They can specifically bind to receptors or antigens present at the target region by attaching particular molecules to the transfer of some surface, raising medication concentration at the targeted place while minimizing systemic exposure.
- **These are lipid-based vesicles that can preserve encapsulated pharmaceuticals against degradation, enzymatic metabolism, and other environmental influences.** This contributes to the drug stability and integrity throughout storage and shipment. This improves medication absorption and bioavailability, resulting in a larger concentration.
- **It provides a non-invasive mode of drug delivery since they may transfer pharmaceuticals via the skin without the need for injections or other intrusive treatments.** This enhances patient compliance and comfort while lowering the risk of infection or other consequences related to invasive treatments.
- **Transfersomes are versatile because they may be made with a range of lipid components, allowing for the customization of their physicochemical features.** This adaptability allows for the development of transfersomes with appropriate properties for certain pharmaceuticals or therapeutic agents such as increased stability, better release kinetics, or extended drug retention.

- Transfersomes provides a number of benefits for transdermal drug administration including greater skin penetration, increased bioavailability, tailored distribution, stability, non-invasiveness, and adaptability. Transfersomes are a potential technique for delivering a wide range of medicines and therapeutic substances via the skin because of these benefits they have the ability to increase transdermal flow and improve bioactive agent site specificity.
- Improving drug bioavailability by avoiding first-pass metabolism which is a fundamental limitation in oral medication delivery.

Disadvantages of Transfersomes

1. **Complexity and Cost:** Transfersome manufacturing entails difficult and costly manufacturing procedures. Transfersome formulation and optimization need specialized equipment and knowledge making their manufacture more difficult as compared to traditional drug delivery methods. Their intricacy and high cost is a limiting factor.
2. **Variable Quality and Consistency:** Its quality and consistency might vary from batch to batch. During the manufacturing process, variations in lipid content, size, and entrapment efficiency may occur, resulting in uneven drug delivery effectiveness. It can be difficult to create uniform and repeatable transfer formulations which limits their use as drug carriers.
3. **Physical Stability Problems:** Transfersomes may experience physical stability problems during storage. They are susceptible to aggregation, fusion, and drug leakage over time. These stability concerns can impair the transfer of some effectiveness and integrity, resulting in alterations in drug release kinetics and a reduction in shelf life.
4. **Scalability Issues:** Moving transfersome manufacturing from the lab scale to the industrial scale might be difficult. To preserve the quality, stability, and efficacy of transfersomes while generating them in higher quantities the production process may need to be optimized. It is difficult to maintain the required features of transfersomes and ~~and~~ consistent performance on a bigger scale.
5. **Toxicity and Immunogenicity:** Transfersomes often contain synthetic or natural phospholipids, which may be poisonous or immunogenic in nature. Although the toxicity and immunogenicity of transfersomes are typically minimal; more research is needed to assure their safety and minimize any side effects.
6. Transfersomes are chemically fragile due to their proclivity for oxidative destruction.
7. Purity of natural phospholipids is another criterion for the use of transfersomes as drug delivery vehicles. [3],[7],[8],[9]

PREPARATION METHOD OF TRANSFERSOMES

Transfersomes are lipid-based vesicles made up of phospholipids and surfactants that allow hydrophilic and lipophilic molecules to be encapsulated. A general approach for preparing transfersomes are:

Each approach is broadly defined as follows:

- **Lipid selection:** Select lipids with excellent deformability and self-assembly characteristics. Commonly utilized phospholipids include phosphatidylcholine, phosphatidylserine, and phosphatidylethanolamine.
- **To make a thin lipid film,** dissolve the specified lipids in an organic solvents combination such as chloroform and methanol. To aid removal in later phases, the solvent combination should be volatile.
- **Solvent removal:** Using a rotary evaporator or a vacuum oven, evaporate the organic solvent under decreased pressure. This process aids in the production of a dry lipid coating on the surface of the container.
- **Rehydration:** Using an aqueous solution containing the medicine or therapeutic substance of interest, rehydrate the lipid film. Based on the drug stability and compatibility, the aqueous solution can be a buffer, saline, or any other acceptable solvent.
- **Sonication:** Mechanically agitate the rehydrated lipid film using an ultrasonic probe or bath sonicator. Sonication aids in the breakdown of the lipid film into tiny vesicles and the creation of transfersomes. To attain the appropriate vesicle size and stability, the duration and intensity of sonication should be optimized.
- **Size reduction:** If the initial vesicles formed are bigger than the intended size range, procedures such as extrusion or high-pressure homogenization can be used to accomplish additional size reduction. These approaches aid in the formation of smaller, more homogenous transfersomes.
- **Purification:** Remove any remaining lipid aggregates, untrapped drugs, or other contaminants from the transfersomes using procedures such as centrifugation or filtering.
- **Characterization** includes determining the transfersomes size distribution, zeta potential, stability,

and drug encapsulation efficiency. This procedure confirms the prepared transfersomes quality and function.

METHODS FOR PREPARATION OF TRANSFERSOMES.

Vortexing sonication method

The sonication vortexing method is a technique for manufacturing transfersomes, to improve medication distribution across biological barriers such as the skin.

Step-by-step instruction for preparing transfersomes with sonication vortexing:

- Formulation ingredients: Phospholipids (such as phosphatidylcholine or phosphatidylserine), a medication or active agent, and any additional desirable additives or stabilizers are required.
- Determine the required quantities of phospholipids and other components based on the intended formulation. These values may differ based on the unique requirements of application.
- Fill an appropriate container, such as a glass vial or tube, with the phospholipids and other components.
- Fill the container with a suitable solvent. Transfersomes are often prepared in chloroform, methanol, or a combination of the two. The solvent used is determined by the lipid content and solubility of the drug or active component.
- Using a vortex mixer thoroughly mix the contents of the container. This step aids in the dissolution of the lipids and the formation of a homogeneous lipid solution. Remove the solvent after producing a homogeneous lipid solution by evaporating it under decreased pressure using a rotary evaporator or by nitrogen gas flow. This procedure is necessary to eliminate any leftover solvent that may have an adverse effect on the stability of the transfersomes.
- Rehydrate the lipid film with a suitable buffer or aqueous solution when the solvent has been entirely evaporated. The choice of a buffer is determined by the drug or active ingredient stability and compatibility criteria.
- Apply sonication to the rehydrated lipid film. Sonication is usually done with an ultrasonic bath or a probe sonicator. Sonication is used to break lipid bilayers and stimulate the development of transfersomes. Adjust the sonication parameters, such as time, intensity, and temperature, based on its unique lipid content and desired qualities. These parameters must be optimized in order to obtain the appropriate vesicle size, stability, and drug encapsulation efficiency.
- Allow the transfersomes to cool and stabilize for a length of time after sonication. This phase promotes lipid bilayer reorganization and the creation of stable transfersomes.[10],[11],[12]

Suspension homogenization process

Suspension homogenization is a common process for preparing transfersomes, which are specialized lipid-based vesicles meant to improve drug transdermal delivery. Transfersomes are made up of phospholipids and edge activators, which provide the property like deformability i.e., required for effective skin penetration.

- The first step is to choose the proper phospholipids and edge activators for the transfersome formulation. Phospholipids such as phosphatidylcholine, phosphatidylethanolamine, and phosphatidic acid are typically utilized, whereas edge activators might include sodium cholate, Tween 80, or Span 80.
- Pre-mixing of phospholipids and edge activators: The phospholipids and edge activators are mixed in the right amounts and dissolved in an organic solvent such as chloroform or ethanol. The lipid phase of the transfersomes solution is formed by this lipid combination.
- Solvent evaporation: Using a rotary evaporator or a vacuum pump, the organic solvent is evaporated at decreased pressure. This technique creates a thin lipid coating on the walls of container for optimum lipid dispersion.
- Hydration: The lipid film is hydrated by progressively introducing an aqueous phase, often a buffer solution to the container. The hydration process permits lipids to self-assemble into vesicles resulting in the formation of transfersomes. Mechanical agitation, such as stirring or shaking can help to encourage the production of vesicles.
- Post-processing: The transfersomes solution is normally filtered through a membrane filter after homogenization to eliminate any leftover large vesicles or aggregates. The filtrate is then collected and its size and stability are assessed using methods such as dynamic light scattering and electron microscopy.

Modified handshaking method

The handshaking approach optimizes the transfer of transfersomes, which are lipid-based vesicles utilized for drug delivery. Transfersomes are made up of phospholipids and edge activators, and they may deform

and pass through small holes. The improved handshaking approach improves transfersome efficiency by encouraging engagement with the target tissue or cells.

The improved handshaking approach is described below:

- Transfersomes are commonly made using either the thin-film hydration approach or the solvent injection method. These procedures include combining the required lipids, such as phospholipids and cholesterol with an organic solvent and then removing the solvent to produce a thin film. To develop transfersomes, the film is hydrated using a suitable aqueous solution.
- Addition of targeting ligands: To improve transfersome specificity for a certain target tissue or cells, targeting ligands can be included in the transfersome formulation. Antibodies, peptides, and other compounds with affinity for specific receptors or markers on target cells are examples of targeting ligands.
- The modified handshaking approach involves a number of procedures to optimize the interaction between transfersomes and the target tissue or cells.
 - a. Preconditioning: The target tissue or cells are preconditioned to produce a favourable environment for transfersome interaction. Treatments may include heating, chilling, or adding specific compounds to the target tissue or cells to increase their receptivity to transfersomes. Transfersomes containing the desired medication or therapeutic agent are transferred to the target tissue or cells. Depending on the application, this can be accomplished by a variety of means such as topical administration, injection, or other acceptable channels.
 - b. Massage or physical stimulation: After the transfersomes are applied, the target tissue or cells are gently massaged or physically stimulated. This can be done manually or using mechanical equipment created expressly for this purpose. The stimulation aids in the interaction of transfersomes with target tissues or cells by boosting transfer by fusion or uptake. [13],[14],[15] Aqueous lipid suspension process

To make an aqueous lipid suspension, lipid molecules are dispersed in water to form a stable and uniform combination. Following is high-level overview of the procedure:

- i) Lipid selection: Select the right lipids, Phospholipids (e.g., lecithin), triglycerides melted or dissolved in an organic solvent depending on the kind of lipid utilised. This process ensures that the lipids scatter freely in water.
- ii) Emulsification is the process of dispersing one liquid phase (lipids) into another liquid phase (water) to produce a stable emulsion. There are numerous approaches to emulsification:
 - a) Swirling at high speed: Place the lipid phase (melted lipids or lipid solution) in a container and gently add the water phase while constantly swirling at high speed. This mechanical force aids in the dispersion of the lipid phase in the water by breaking it up into minute droplets.
 - b) Homogenization: Force the lipid and water phases through a tiny nozzle or valve at high pressure using a high-pressure homogenizer. This procedure reduces the size of the lipid droplets and guarantees homogeneous dispersion.
 - c) Sonication: Using a sonicator apply ultrasonic waves to the mixture. The pressure changes caused by the high-frequency sound waves break down the lipid phase into smaller droplets, increasing their dispersion in the water. [2],[3],[16],[17],[18]

Centrifugation Process

This process involves dissolving phospholipids, surfactants, and medication in alcohol. The alcohol is then evaporated using rotary evaporation at 40°C and reduced pressure to remove the solvent residues. Vacuum is applied to ensure the complete removal of any remaining solvent. The resulting lipid film is hydrated by adding the appropriate buffer and centrifuging at room temperature for 1 hour at 60 rpm. Following hydration, the vesicles are allowed to inflate for 2 hours at room temperature. Finally, the multi-lamellar lipid vesicles are sonicated at normal temperatures. [19] Characterization of the Transfersomes

Vesicle Size, Zeta Potential, and Morphology:

While production, batch-to-batch comparison, and scale-up processes, the vesicle size is a significant issue to consider. The altering vesicle size during storage is a key component in the physical stability of formulation. Because of the high curvature state of their bilayer membranes, vesicles smaller than 40 nm are prone to fusion processes whereas much bigger and electroneutral transfersomes connect via van der Waals contacts due to significantly wider membrane contact areas. Transfersomes capacity to encapsulate drug substances is influenced by vesicle size. While lipophilic and amphiphilic agents prefer a high lipid-to-core ratio, hydrophilic chemical encapsulation favours a greater aqueous core volume. In general, dynamic light scattering (DLS) enables the vesicle suspension to be combined with a suitable medium and vesicular size

measurements to be performed in triplicate. As an alternative method the sample is prepared in distilled water and filter it using a 0.2 mm membrane filter. The filtered sample is then diluted with filtered saline to determine vesicle size using DLS or PCS. Furthermore, the computerized inspection system connected with the Malvern Zettaliter DLS technique may be used to measure vesicle size and size distribution, while transmission electron microscopy (TEM) can be utilized to discover structural abnormalities. The electrophoretic mobility technique is used to calculate the zeta potential using the Malvern Zettaliter. The transfer of specific vesicles can be seen via TEM or phase contrast microscopy.[19]

Number Of vesicles per cubic mm:

This value is critical for optimizing the transfer of transfersomes in certain compositions as well as other process factors. Transfersome formulations that were not prepared are diluted five times with 0.9% sodium chloride. This sample is evaluated using a Hemocytometer and an optical microscope. An optical microscope can identify transfersomes with vesicle sizes larger than 100 nm. The following formula is used to compute the number of transfersomes in tiny squares:

Total number of Transfersomes per cubic mm

$$= \frac{(\text{Total Number of Transfersomes counted} \times \text{dilution factor} \times 4000)}{\text{Total number of squares counted}}$$

Entrapment Efficiency (%)

The amount of drug entrapped in the formulation is represented by the percentage of entrapment efficiency (%EE). The EE is derived by separating the untrapped drug from the vesicles using a variety of methods, including mini-column centrifugation. The %EE can be calculated using either direct or indirect approaches in this procedure. The supernatant would be removed after ultracentrifugation, and the sedimented vesicles would be disturbed with a suitable solvent capable of lysing the sediment. Dilute the solution and filter it using a syringe filter (0.22-0.45 m) to eliminate the contaminants. The drug concentration is determined using analytical methods such as modified high-performance liquid chromatography (HPLC) or spectrophotometry, depending on the active pharmaceutical ingredient (API) analytical method. [20]

Deformability Level

This is a significant factor since it affects the transfersome formulation's penetration. The criteria for this deformity level is pure water. A series of microporous filters with known pore diameters ranging from 50 to 400 nm are used to filter the mixture. DLS data are used after each pass to measure particle size and size distribution. The degree of deformability is expressed by:

$$D = J(r_v/r_p)$$

where D is the degree of deformability, J is the amount of suspension extruded in 5 minutes, r_v is vesicle size, and r_p is barrier pore size.

In Vitro Drug Release

The *in-vitro* drug release profile may provide important information on formulation design as well as data on release mechanism and kinetics, enabling a scientific approach to optimizing the transfersome formulation. The *in-vitro* drug release of transfersomes is often compared to that of the free drug or reference product. Many studies on the pharmacological release patterns of well-established transfer-specific formulations have generated encouraging results. After 6 hours, celecoxib transfersome gel revealed 75% drug release, a 30% increase above the commercial gel. After 6 hours, ketoconazole-loaded transfersome gel had a higher first burst of drug release (40.67%) than ketoconazole solution (27.35%). In the *in vitro* release profile of lidocaine from transfersome vesicles, more than 80% of the drug was released after 6 hours. Franz diffusion cells are employed in studies of *in-vitro* drug release. Adhesive tape holds the donor chamber together. The fluid in the receptor chamber is constantly stirred by a magnetic bar. During the release experiment, the receptor fluid should be kept at the typical *in vivo* skin surface temperature of 32 ± 1 °C. A mixed cellulose ester membrane with an average pore size of 0.45 m is used with release media (phosphate buffer) overnight at room temperature. To keep the sink conditions, aliquots of 1 mL of the receptor media are taken at appropriate time intervals (such as 0, 0.5, 1, 2, 3, 4, 5, and 6 h) and replaced with an equal volume of fresh PBS. The gathered samples can be evaluated using appropriate techniques.[21]

In-Vitro Skin Permeation Studies

It is carried out to establish the transport efficiencies of transdermal administration systems and to find the elements that promote drug transdermal flux which is commonly reported in units of g/cm²/h. The results of this study may potentially be used to anticipate *in-vivo* behaviors from various transdermal delivery methods and to optimize the formulation prior to perform more expensive *in-vivo* investigations. The human skin should ideally be utilized to evaluate the permeability qualities of proposed formulations.

However, the human skin limited available, ethical issues, and religious limitations make it less appealing for permeation research. Primate, porcine, rat, mouse, guinea pig, and snake skins have all been proposed as more accessible alternatives for human skin. It should be emphasized. However, that percutaneous absorption via different animal skins might differ dramatically from those obtained with human skin models. According to the published data pig skin is clearly the most suitable animal model for human skin because the fluxes through the skin as well as the concentrations in the skin, were shown to be of the same order of magnitude for both of those tissues with minor differences of no more than two or four-fold, respectively [98]. Furthermore synthetic membranes (i.e; Strat_M membrane) have been used in transdermal permeation investigations as an alternative. Synthetic membranes have been shown to have extremely near similarities to human skin. In compared to human and animal skins, this model has the benefit of being more constant in permeability and reactivity. Franz diffusion cells are used for skin permeation investigation. The membranes are horizontally positioned on the receptor compartments with the stratum corneum pointing upwards towards the donor compartments. The Franz diffusion cells receptor compartments are filled with phosphate buffer saline solution which is agitated by a magnetic bar. Because the receptor fluid is intended to simulate blood circulation beneath the skin, it should be maintained around 37 ± 0.5 °C. An acceptable amount of the testing formulation is added into each donor compartment as it is placed on the membrane, and the top of the diffusion cell is opened to mimic nonoccluded conditions. Specific volumes of aliquots of the receptor medium are withdrawn at appropriate time intervals, and simultaneously, the receptor medium is replaced by an equal volume of the fresh receptor medium to maintain the sink conditions. The obtained samples can be analyzed by HPLC or the spectroscopic method. [22],[23],[24]

Stability of Transfersomes

Transfersome vesicles shape and size may be monitored over time to evaluate their stability. DLS and TEM may be used to calculate mean size and structural changes, respectively. The improved transfersome formulations can be kept at various temperatures in hermetically sealed amber vials. According to ICH guidelines, the general case for storage conditions for new drug substances and products is 25 ± 2 °C/60% relative humidity (RH $\pm 5\%$ RH or 30 ± 2 °C/65% RH $\pm 5\%$ for 12 months and 40 ± 2 °C/75% RH $\pm 5\%$ for six months for accelerated testing for medication products planned for refrigeration, long-term storage at 5 ± 3 °C for 12 months and accelerated research at 25 ± 2 °C/60% RH 5% RH for six months.[1],[25],[26]

FUTURE ASPECTS OF TRANSFERSOMES

Transfersomes are lipid-based vesicles that have received attention in the field of medication administration due to their unique features. They are made of phospholipids and may encapsulate both hydrophilic and hydrophobic drug. Transfersomes have the capacity to bend and squeeze through small holes, allowing for greater penetration through biological barriers such as the skin.

In terms of the future, transfersomes have enormous promise in a variety of areas:

- Transfersomes are effective NDDS in terms of drug delivery. Their deformability and flexibility allow for effective penetration into deeper layers of the epidermis, improving transdermal medication administration. This characteristic offers opportunities for the treatment of numerous dermatological disorders as well as systemic medication administration.
- Cosmetics and Personal Care: Transfersomes are used in the cosmetics and personal care industries. Their capacity to penetrate the skin barrier can be used to target specific layers of the skin with cosmetic chemicals such as anti-aging compounds or skin-whitening agents. Transfersomes may potentially improve the transport of UV filters in sunscreen compositions, increasing their effectiveness.
- Transfersomes can be utilized as carriers for targeted medication delivery to specific cells or tissues in nanomedicine. They can carry medications directly to the targeted region by altering the surface of transfersomes with ligands or antibodies that precisely attach to receptors on target cells. This strategy has the potential to increase treatment efficacy while minimizing negative effects.
- Transfersomes have the potential to be used as carriers for gene therapy. They can encapsulate and transmit genetic material, such as plasmid DNA or RNA to target cells. Transfersome deformability enables the effective transport of genetic material across cell membranes providing a viable strategy for gene therapy applications.
- Transfersomes can be used in combination treatments in which many medications or therapeutic agents are administered at the same time. The capacity of transfersomes to encapsulate both hydrophilic and hydrophobic medicines enables the co-delivery of synergistic drug combinations, improving therapeutic effects.

- Bioimaging: For diagnostic purposes transfersomes can be loaded with imaging agents such as fluorescent dyes or nanoparticles. It is feasible to see specific tissues or monitor the biodistribution of drug-loaded transfersomes in real-time by adding imaging agents into transfersomes assisting in the development of personalized medicine.[27],[28],[29].

LIMITATIONS OF TRANSFEROSOMES

- Transfersomes, a kind of lipid-based vesicle, have various benefits as drug delivery vehicles, including increased skin permeability, greater stability, and formulation flexibility. They do, however, have certain limits. Here are a few examples:
- Formulation complexity: Transfersomes preparation requires the use of specialized processes such as sonication or extrusion, which may be technically demanding and time-consuming. Transfersome formulation optimization necessitates knowledge and may involve several trial-and-error processes.
- Transfersomes are prone to physical and chemical instability, which can result in aggregation, fusion, and drug leakage. Temperature, pH, and mechanical stress can all have an impact on their stability. This can limit their long-term storage, shelf life, and drug delivery efficacy.
- Transfersomes can have a wide size variation ranging from 10-100nm. This variation in size has the potential to impact their penetration into target tissues and cells and their overall efficacy as drug transporters.
- Low encapsulation efficiency: It might be difficult to achieve high encapsulation efficiency, i.e., incorporating a large amount of drug into transfersomes. Some medications may have limited solubility in the lipid bilayers of transfersomes or show vesicle leakage resulting in decreased drug loading.
- Drug compatibility is limited: Not all drugs can be encapsulated in transfersome. Some medications may interact with the lipid components, reducing their stability or effectiveness. Furthermore, the encapsulation procedure may change the physicochemical characteristics of the drug, influencing its therapeutic effect.
- Restore response transfersomes manufactured at large volumes can be problematic because of the intricacy of the formulation process and the requirement for specialized equipment. It might be difficult to scale up the production process while keeping its necessary features. [30-35]

CONCLUSION

Transfersomes as lipid based nanocarrier are frontrunners in transdermal drug delivery. It offers several advantages compared to other routes of administration such as oral or injectable methods. One advantage is that a lower daily dose of the drug can often be used while still achieving an equivalent therapeutic effect. This is because the drug is absorbed directly through the skin and bypasses the digestive system and first-pass metabolism in the liver which can reduce the required dosage. In emergency situations where a patient is unresponsive or unconscious; it can be easily and rapidly delivered and identified due to their physical presence on the skin that makes it easier for medical personnel to identify the medication being administered and take appropriate action. The suitability of this route of administration depends on various factors including the specific medication, the patient condition and individual considerations. Newer formulations will definitely help to achieve predicted drug delivery with minimal dosage frequency and side effects.

REFERENCES

1. Opatha SA, Titapiwatanakun V, Chutoprapat R. (2020). Transfersomes: A promising nanoencapsulation technique for transdermal drug delivery. *Pharmaceutics*. ;12(9):855.
2. Shuwaili AH, Rasool BK, Abdulasool AA. (2016). Optimization of elastic transfersomes formulations for transdermal delivery of pentoxifylline. *European Journal of Pharmaceutics and Biopharmaceutics*. 1;102:101-14.
3. Rai S. & Dubey, N. (2023). Regulatory control over chewable gels and current challenges. *Ann. Phytomed.*,12(1):1-8.
4. Mahmood S, Taher M, Mandal UK. (2014). Experimental design and optimization of raloxifene hydrochloride loaded nanotransfersomes for transdermal application. *International journal of nanomedicine*. 12:4331-46.
5. Jain AK, Kumar F. (2017). Transfersomes: Ultradeformable vesicles for transdermal drug delivery. *Asian J. Biomater. Res.* ;3:1-3.
6. Xu X, Khan MA, Burgess DJ. (2012). Predicting hydrophilic drug encapsulation inside unilamellar liposomes. *International journal of pharmaceutics*. 28;423(2):410-8.8
7. Ge X, Wei M, He S, Yuan WE.(2019). Advances of non-ionic surfactant vesicles (niosomes) and their application in drug delivery. *Pharmaceutics*. 29;11(2):55.
8. Mujoriya RZ, Dhamande K, Bodla RB. (2011). Niosomal drug delivery system—a review. *Int j appl pharm.*

- 28;3(3):7-10.
9. Touitou E, (1996). Compositions for applying active substances to or through the skin. United States patent US 5,540,934.
 10. El Sayyad MK, Zaky AA, Samy AM. (2017). Fabrication and characterization of sildenafil citrate loaded transfersomes as a carrier for transdermal drug delivery. *Pharm.Pharmacol. Int. J.* 5:37-46.
 11. Baldrick P. (2000). Pharmaceutical excipient development: the need for preclinical guidance. *Regulatory toxicology and pharmacology.* 1;32(2):210-8.
 12. Pirvu CD, Hlevca C, Ortan A, Prisada R. (2010). Elastic vesicles as drugs carriers through the skin. *Farmacia.* 1;58(2):128-35.
 13. Duangjit S, Opanasopit P, Rojanarata T, Ngawhirunpat T. (2011). Characterization and in vitro skin permeation of meloxicam-loaded liposomes versus transfersomes. *Journal of drug delivery.* 20: 11.
 14. El Maghraby GM, Williams AC, Barry BW. (2000). Skin delivery of oestradiol from lipid vesicles: importance of liposome structure. *International journal of pharmaceutics.* 20;204(1-2):159-69.
 15. Liska DA, Akucewich LH, Marsella R, Maxwell LK, Barbara JE, Cole CA. (2006). Pharmacokinetics of pentoxifylline and its 5-hydroxyhexyl metabolite after oral and intravenous administration of pentoxifylline to healthy adult horses. *American journal of veterinary research.* 1;67(9):1621-7.
 16. Langer R. (2004). Transdermal drug delivery: past progress, current status, and future prospects. *Adv. Drug. Deliv. Rev.* 56:557-8.
 17. Honeywell-Nguyen PL, Bouwstra JA. (2005). Vesicles as a tool for transdermal and dermal delivery. *Drug discovery today: technologies.* 1;2(1):67-74.
 18. Subedi RK, Oh SY, Chun MK, Choi HK. (2010). Recent advances in transdermal drug delivery. *Archives of Pharmacol Research.* 33:339-51.
 19. Singh N.K. & Dubey, N. (2013). Cleaning validation: regulatory expectations and methodological challenges. *Eur. Chem. Bull.* 12(4):15137-15164.
 20. Yavlovich A, Singh A, Blumenthal R, Puri A. (2011). A novel class of photo-triggerable liposomes containing DPPC: DC8, 9PC as vehicles for delivery of doxorubicin to cells. *Biochimica et Biophysica Acta (BBA)- Biomembranes.* 1;1808(1):117-26.
 21. Prajapati ST, Patel CG, Patel CN. (2011). Transfersomes: A vesicular carrier system for transdermal drug delivery. *Asian Journal of Biochemical and Pharmaceutical Research.* ;2(1):507-24.
 22. Cevc G, Blume G, Schätzlein A. (1997). Transfersomes-mediated transepidermal delivery improves the regio-specificity and biological activity of corticosteroids in vivo. *Journal of controlled release.* 7;45(3):211-26.
 23. Hui-hui Z, qiu-hua L, zhi-jun Y, wei-san P, shu-fang N. (2011). Novel ophthalmic timolol mealeate liposomal-hydrogel and its improved local glaucomatous therapeutic effect in vivo. *Drug Delivery.* 1;18(7):502-10.
 24. Maiti S, Paul S, Mondol R, Ray S, Sa B. (2011). Nanovesicular formulation of brimonidine tartrate for the management of glaucoma: in vitro and in vivo evaluation. *Aaps Pharmscitech.* 12:755-63.
 25. Achouri D, Alhanout K, Piccerelle P, Andrieu V. (2013). Recent advances in ocular drug delivery. *Drug development and industrial pharmacy.* 1;39(11):1599-617.
 26. Fathalla D, Soliman G, Fouad E. (2015). Development and in vitro/in vivo evaluation of liposomal gels for the sustained ocular delivery of latanoprost. *J Clin Exp Ophthalmol.* 6(390):2.
 27. Fitzgerald P, Hadgraft J, Kreuter J, et al. (1987). A γ -scintigraphic evaluation of microparticulate ophthalmic delivery systems: liposomes and nanoparticles. *Int J Pharm.* 40(1-2):81-84.
 28. Chourasia MK, Kang L, Chan SY. (2011). Nanosized ethosomes bearing ketoprofen for improved transdermal delivery. *Results in pharma sciences.* 1;1(1):60-7.
 29. Ahad A, Aqil M, Kohli K, Sultana Y, Mujeeb M, Ali A. (2012). Formulation and optimization of nanotransfersomes using experimental design technique for accentuated transdermal delivery of valsartan. *Nanomedicine: nanotechnology, biology and medicine.* 1;8(2):237-49.
 30. Saxena, S., Jain A. & Dubey, N. (2023). Quality by Design Approaches for The Optimization of Oral Disintegrating Film. *Adv. Biores.* 14(5). EISSN: 2377 - 1573.
 31. Patel, G., Bhadoriya U. & Dubey, N. (2023). Role of Statistics Based Software's for the Optimization of Pharmaceutical Formulations. *Adv. Biores.*, [In-press]
 32. Singh, T., Jain A. & Dubey, N. (2023). A Qualitative Approach to Wurster based Pellet and Coating Technique. *Adv. Biores.* 14(5). EISSN: 2377 - 1573.
 33. Khajeh M. Application of Box-Behnken design in the optimization of a magnetic nanoparticle procedure for zinc determination in analytical samples by inductively coupled plasma optical emission spectrometry. *Journal of Hazardous Materials.* 2009 Dec 15; 172(1):385-9.
 34. Vaddi HK, Ho PC, Chan YW, Chan SY. Oxide terpenes as human skin penetration enhancers of haloperidol from ethanol and propylene glycol and their modes of action on stratum corneum. *Biological and Pharmaceutical Bulletin.* 2003; 26(2):220-8.
 35. Mihaulia P. & Dubey, N. (2013). 3D Printing As A Novel Formulation Tool: A Regulatory Perspective. *Eur. Chem. Bull.* 12(4):15137-15164.

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